

Advanced Feature Selection in Multinomial Dementia Classification from Structural MRI Data

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Introduction

A major challenge in Neuroscience¹ is the discovery of the best subset of biomarkers that could improve the accuracy in discriminating Alzheimer's disease from the Mild Cognitive Impairment.

MRI Datasets and Feature Generation

Feature extraction from MRIs performed by FreeSurfer²:

- ◆ 45 volumes of subcortical structures;
- ◆ 34 mean thickness and 34 cortical volumes for each hemisphere;
- ◆ 8 hippocampus volume subfields for each hemisphere;

for a total of **200 attributes** including the diagnosis, gender and age.

The ADNI dataset (D2, Table 1) includes those subjects:

- ◆ diagnosed as healthy control (HC), Alzheimer's disease (AD) and late Mild Cognitive Impairment (late MCI);
- ◆ that completely passed the quality test;
- ◆ that have *Non-Accelerated T1* scans related to the baseline visit.

Table 1. Descriptive statistics of the CADDementia and ADNI data sets. Age values (years) are mean±standard deviation and include both female and male subjects.

Description	Name	Class	Nr. of subjects	Female%	Age (mean±std)
CADDementia training set	D1	HC	12	25%	62.33±6.26
		AD	9	66.6%	66.11±5.21
		MCI	9	44.4%	68±8.54
ADNI	D2	HC	70	48.6%	73.6±5.49
		AD	70	52.8%	74.15±8.07
		MCI	70	45.7%	72.6±7.78

Feature Selection and Classification Model Inference

Feature selection³ can reduce dimensionality, thus mitigating computational performance issues and improving the classification accuracy.

The adopted workflow is composed by five steps (Fig. 1):
(i) *IntraCranial Volume* normalization; (ii) *Feature Selection* with three techniques; (iii) *Z-Score normalization*; (iv) binary classification and (v) multi-class classification (*one-versus-one*).

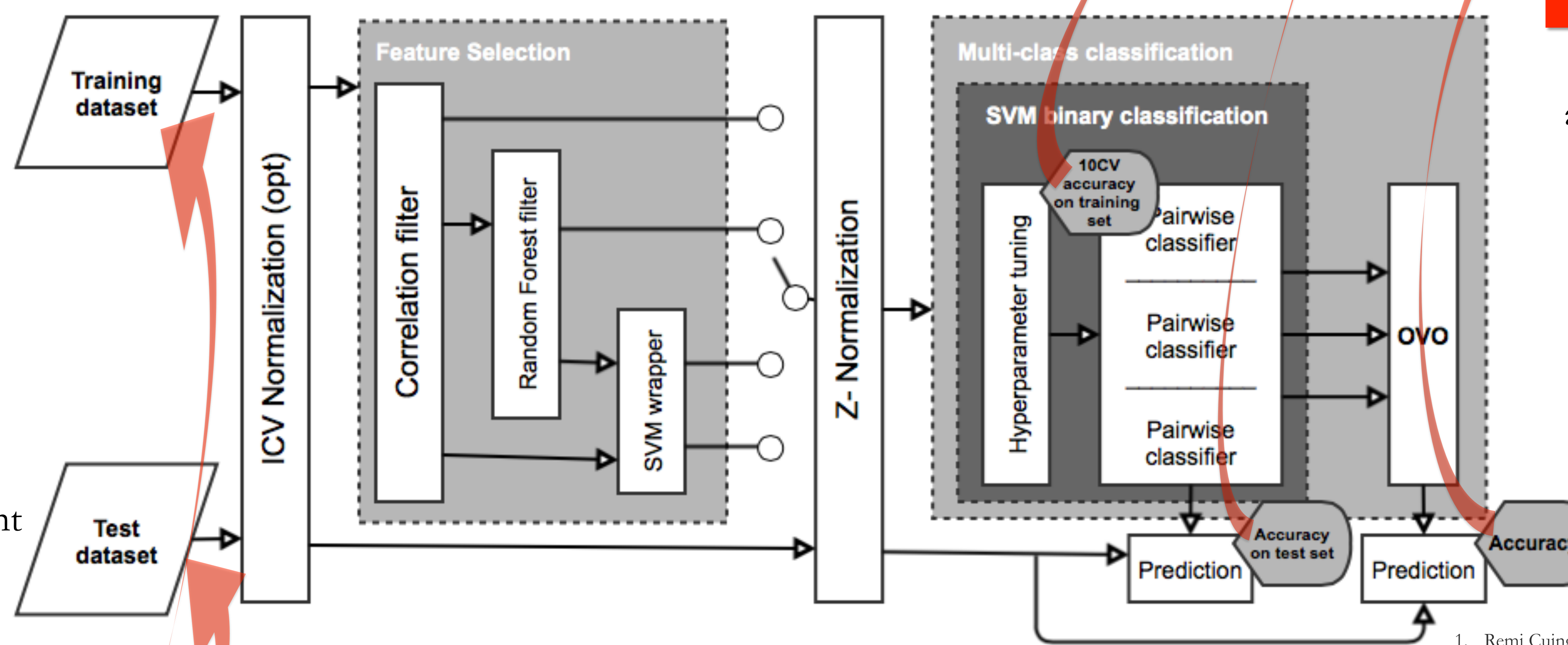


Fig. 1 Diagram of the adopted workflow based on a combination of feature selection techniques.

The core of the proposed method consists in sequentially applying a Correlation filter, a Random Forest (RF) filter and a Support Vector Machines (SVM) wrapper on the training dataset, to identify a subset of features that provides the highest binary classification accuracy (Table 2 and 3).

The three best binary classification models have been used for performing the multi-class classification.

Results

Table 2. Results of the binary classification: training performed on D2 and accuracy estimated on D2 (D2/D2) and D1 (D2/D1). Best results on D1 are indicated in bold.

	Feature selection method											
	Corr. filter r <0.90			Random Forest filter			SVM wrapper			Random Forest filter + SVM wrapper		
	ICV	No ICV		ICV	No ICV		ICV	No ICV		ICV	No ICV	
	Nr.	D2/D2	D2/D1	Nr.	D2/D2	D2/D1	Nr.	D2/D2	D2/D1	Nr.	D2/D2	D2/D1
	10xval	holdout	feat.	10xval	holdout	feat.	10xval	holdout	feat.	10xval	holdout	feat.
HCvsMCI	133	71.4%	42.9%	140	67.9%	66.7%	71	71.4%	42.9%	41	65.7%	52.4%
HCvsAD	133	90%	42.9%	140	81.4%	90.2%	109	86.4%	42.9%	95	82.1%	95.2%
ADvsMCI	133	58.6%	50%	139	58.6%	83.3%	47	60%	50%	44	62.1%	88.9%

Table 3. Results of multi-class classification. The VOTE strategy for the *one-versus-one* classification has been applied on datasets with and without IntraCranial Volume normalization.

OVO accuracy	
ICV normalization	30%
No ICV normalization	70%

Table 4. Mean computation time for each step of the proposed approach.

Step	Time
ROI feature extraction	5 hours per subject
Correlation filter	0.836 s
Random Forest filter	7.744 s
SVM wrapper	112.790 s
RF filter + SVM wrapper	91.790 s
OVO classification	0.496 s

Conclusions

The present study was designed for exploring and evaluating alternative subsets of ROI features extracted by FreeSurfer from brain MRIs, by applying advanced methods for feature selection.

The findings suggest that (i) ICV normalization can lead to overfitting and worse accuracy and (ii) even though the SVM wrapper is more complex and slower than the Random Forest filter, it does not provide better accuracy.

References

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